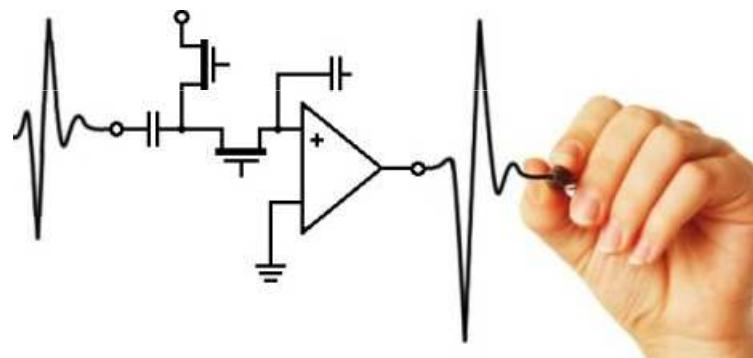


# Semi-Empirical Optimization of CMOS Low-noise Amplifier for Biomedical Data Acquisition



MAGNANIL GOSWAMI  
PROF. SUDAKSHINA KUNDU



# Contents

---

- Prologue
- Amplifier for Biomedical Data Acquisition
- Optimization Methodology:
  - Orthogonal-Convex Optimization
  - All-Inversion Region MOS Model
- Design Formulation
- Result Interpretation
- Epilogue



# Prologue

---

- Design of neural recording interfaces.  
[for biomedical measurements]
- Generic structure of neural recording interfaces.
- Low-Noise Amplifier (LNA): A Key Element.
- Design challenge.  
[stringent noise-power-area trade-off ]
- Application domain of biomedical LNAs.  
[ECG, EEG, EMG]



# Amplifier for Biomedical Data Acquisition

- Capacitive feedback network (CFN) topology.
- Prerequisites.
  - low power, low input-referred noise and high CMRR
- ❤️ of the CFN LNA: Preamplifier.

Table 1

Signal	Frequency (Hz)	Amplitude (V)
ECG	0.05 – 250	$5 \times 10^{-6} – 8 \times 10^{-3}$
EEG	0.5 – 200	$2 \times 10^{-6} – 200 \times 10^{-6}$
EMG	0.01 – 10 $\times 10^3$	$50 \times 10^{-6} – 10 \times 10^{-3}$

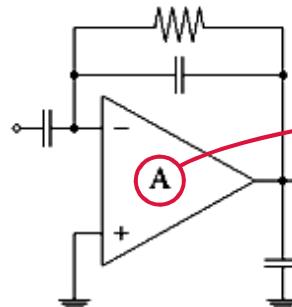


Figure 1

Transfer function  $\approx$  
$$\frac{\text{open-loop voltage gain}}{\left[1 + \frac{s}{-\text{dominant pole}}\right] \left[1 + \frac{s}{-\text{output pole}}\right] \left[1 + \frac{s}{-\text{compensation pole}}\right]}$$

Figure 2

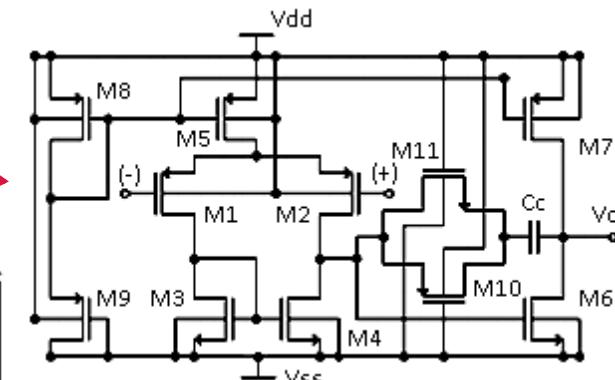
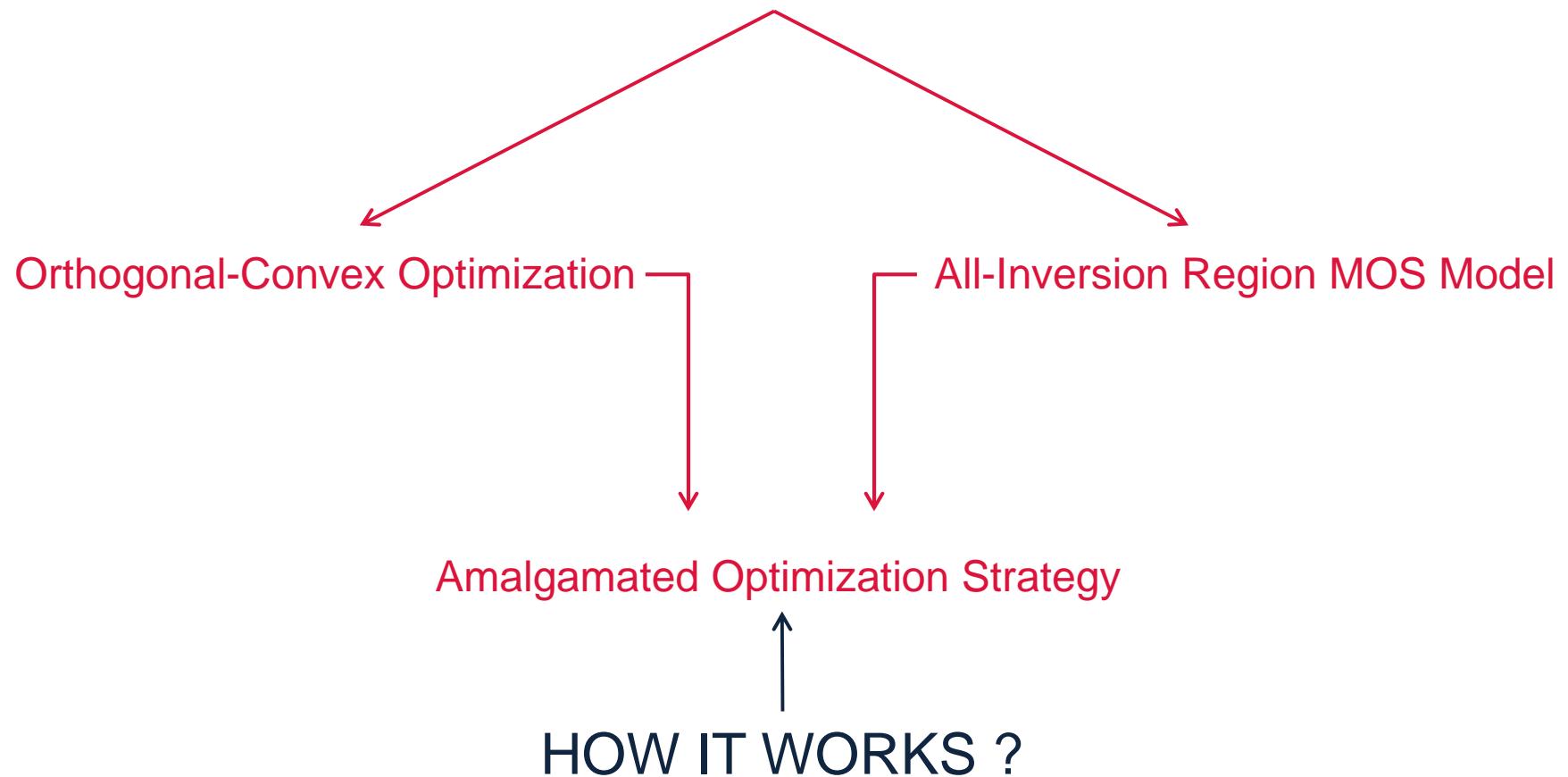


Figure 3



# Optimization Methodology



continued in next slide...



...from previous slide

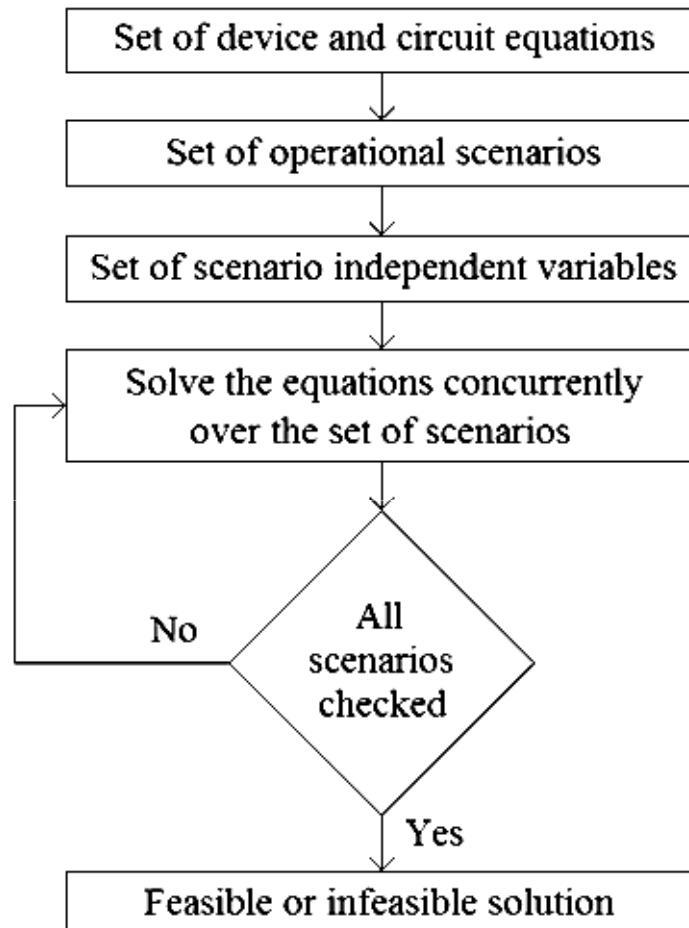


Figure 4

continued in next slide...



...from previous slide

---

## Orthogonal-Convex Optimization

- Objective & Constraint Based Optimization.
- Problem Formulation:

$$\begin{aligned} & \text{optimize } f_0(x) \\ & \text{subject to } f_i(x) \leq 1, \quad i = (1, \dots, m) \\ & \quad g_i(x) = 1, \quad i = (1, \dots, p) \\ & \quad x_i > 0, \quad i = (1, \dots, n) \end{aligned}$$

- Monomial & Posynomial:

$$g(x) = cx_1^{a_1} \dots x_n^{a_n} \quad f(x) = \sum_{k=1}^K c_k g_k(x)$$

- Logarithmic Transformation of Variables.

continued in next slide...

---



...from previous slide

---

## All-Inversion Region MOS Model

- Inversion Coefficient of MOSFET Optimization.

$$ICF = \frac{I_D}{I_0 S}$$

$$I_0 = 2n\mu C_{ox} \phi_T^2$$

Weak Inversion:  $ICF < 0.1$   
Strong Inversion:  $ICF > 10$   
Moderate Inversion:  $0.1 < ICF < 10$

- Transconductance Efficiency.

$$\frac{g_m}{I_D} = \frac{1}{n\phi_T} \frac{2}{(1 + \sqrt{ICF + 1})}$$



# Design Formulation

---

- Objective: Minimize Power Dissipation
- Constraints:
  - gain-bandwidth, voltage gain, common-mode rejection ratio, slew-rate, phase margin, noise spectral density
- Upper and/or Lower Bounds on Design Parameters.
- Example 1:

Open-loop Gain = Gain of 1<sup>st</sup> Stage x Gain of 2<sup>nd</sup> Stage

$$\begin{aligned} &= \left( \frac{g_{m2}}{g_{o2} + g_{o4}} \right) \left( \frac{g_{m6}}{g_{o6} + g_{o7}} \right) \\ &= \frac{\left( \frac{g_{m2}}{I_{D2}} I_{D2} \right)}{\left( \frac{I_{D2}}{V_{A2}} + \frac{I_{D4}}{V_{A4}} \right)} \frac{\left( \frac{g_{m6}}{I_{D6}} I_{D6} \right)}{\left( \frac{I_{D6}}{V_{A6}} + \frac{I_{D7}}{V_{A7}} \right)} \end{aligned}$$

continued in next slide...

---



...from previous slide

---

## ■ Example 2:

$$\text{Nulling Active Resistor} = R_z$$

$$= \frac{1}{g_{m6}}$$

$$= \frac{1}{\frac{g_{m6}}{I_{D6}} I_{D6}}$$

Table 2

## ■ Design Summary:

[180-nm BSIM3 CMOS Model]

Transistor length	0.18μm ≤ L ≤ 1.8μm
Device width	0.18μm ≤ W ≤ 180.0μm
Supply voltage	1.25V
Load capacitance	1pF
Oxide thickness	4.1nm
Open-loop voltage gain	≥ 60dB
Common-mode rejection ratio	≥ 60dB
Gain-bandwidth	≥ 1MHz
Slew-rate	≥ 1V/μS
Phase margin	≥ 60°
Input-referred noise	≤ 450nV/√Hz
Power	Minimize



# Result Interpretation

---

- 2-Tier Process: Estimation and Verification.

Table 3

Transistor length	$L_1=L_2$ $L_3=L_4$ $L_5=L_7=L_8$ $L_6$	1.8μm 1.8μm 1.43658μm 1.8μm
Transistor width	$W_1=W_2$ $W_3=W_4$ $W_5$ $W_6$ $W_7$ $W_8$	180μm 180μm 180μm 20.87414μm 10.43707μm 1.43658μm
Nulling active resistance	$R_Z$	420.7278kΩ
Compensation capacitance	$C_C$	1.780275pF
Open-loop voltage gain	$G$	80.0dB
Common-mode rejection ratio	$CMRR$	82.70868dB
Gain-bandwidth	$GBW$	22.44995MHz
Slew-rate	$SR$	1V/μS
Phase margin	$PM$	78.07401°
Input-referred noise	$S_{in}(f)$	319.6656nV/√Hz
Power	$P$	64.8477μW

continued in next slide...



...from previous slide

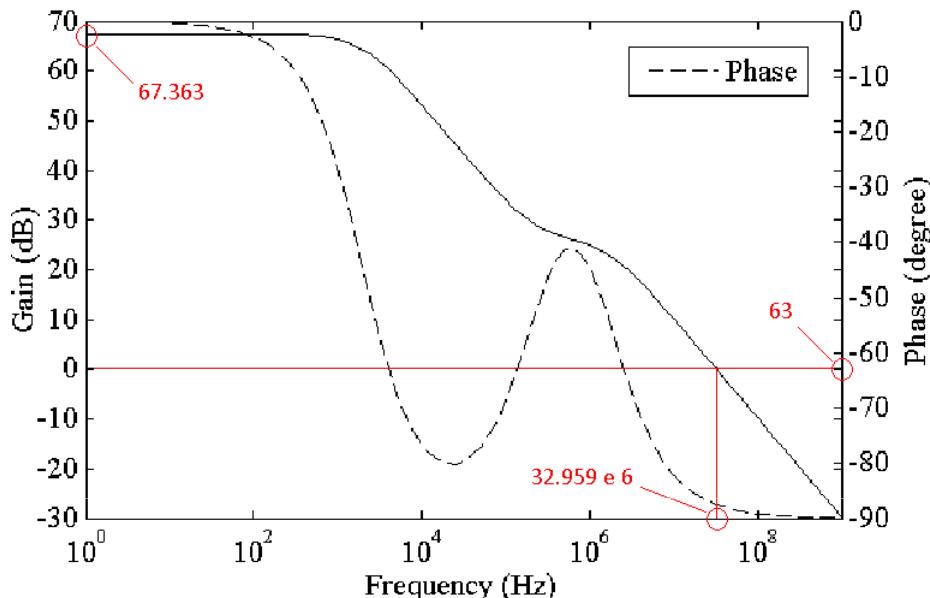


Figure 5

Table 4

Parameter	This method	SPICE	Unit
$G$	80.0	67.363	dB
$CMRR$	82.70868	94.124	dB
$GBW$	22.44995	32.959	MHz
$SR$	1	1.45	V/ $\mu$ S
$PM$	78.07401	63	degree
$P$	64.8477	64.8476	$\mu$ W

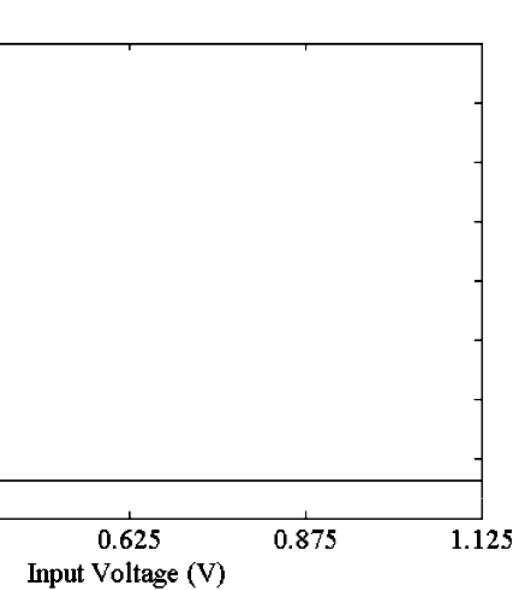


Figure 6

# Epilogue

- Amalgamated Optimization Strategy:

***effectiveness*** of Orthogonal-Convex Optimization

+

***flexibility*** of All-Inversion MOSFET Model

- Pertains Prompt & Globally Optimal Solutions. 
- Increased Fidelity and Flexibility of Design. 
- Rigorous Initial Computation. 
- Limited Function Handling Capability. 



"Further Accuracy is Achievable by Adopting Judicious Design Strategies"



# References

---

- [1] A. M. Sodagar, G. E. Perlin, Y. Yao, K. Najafi, "An implantable 64-channel wireless microsystem for single-unit neural recording," *IEEE J. Solid-State Circ.*, vol. 44, pp. 2591–2604, Sep. 2009.
- [2] M. S. Chae, Z. Yang, M. R. Yuce, L. Hoang, W. Liu, "A 128-channel 6 mW wireless neural recording IC with spike feature extraction and UWB transmitter," *IEEE Trans. Neural syst. & rehab. eng.*, vol. 17, pp. 312–321, Aug. 2009.
- [3] R. R. Harrison, et al: "Wireless neural recording with single low-power integrated circuit," *IEEE Trans. neural syst. & rehab. eng.*, vol. 17, pp. 322–329, Aug. 2009.
- [4] W. S. Wang, Z. C. Wu, H. T. Huang, C. H. Luo, "Low power instrumental amplifier for portable ECG," *IEEE Circ. and Sys. International Conference*, pp. 1–4, 2009.
- [5] C. T. Ma, P. I.Mak, M. I.Vai, P. Mak, S. H. Pun, W. Feng, R. P. Martins, "A 90nm CMOS bio-potential signal readout front-end with improved powerline interference rejection," *IEEE Circ. and Sys.*, pp. 665–668, 2009.
- [6] B. Gosselin, M. Sawan, C. A. Chapman, "A low-power integrated bioamplifier with active low-frequency suppression," *IEEE Trans. Biomed. Circ. & Syst.*, vol. 1, pp. 184–192, Sep. 2007.
- [7] R. R. Harrison, C. Charles, "A low-power low-noise CMOS amplifier for neural recording applications," *IEEE J. Solid-State Circ.*, vol. 38, no. 3, pp. 958–965, June 2003.
- [8] W. Zhao, H. Li, Y. Zhang, "A low-noise integrated bioamplifier with active DC offset suppression," *IEEE Trans. Biomed. Circ. & Syst.*, pp. 5–8, Nov. 2009.
- [9] W. Wattanapanitch, M. Fee, R. Sarpeshkar, "An energy-efficient micropower neural recording amplifier," *IEEE Trans. Biomed. Circ. & Syst.*, vol. 1, pp. 136–147, Jun. 2007.
- [10] R. Stein, B. Charles, D. Davis, L. Jhamandas, J. A. Mannard and T. R. Nichols, "Principles underlying new methods for chronic neural recording", *Can. J. of Neuro. SCI.*, pp. 235–244, 1975.
- [11] D. Popovic, B. Stein, R. B. Jovanovic, K. L. Dai, A. R. Kostovand, W. W. Armstrong, "Sensory nerve recording for closed-loop control to restore motor function," *IEEE Trans. Biomed. Eng.*, vol. 40, no. 10, pp. 1024–1031, 1993.
- [12] Y. Hu, M. Sawan, "CMOS front-end amplifier dedicated to monitor very low amplitude signal from implantable sensors," *Kluwer Academic Publishers*, vol. 33, pp. 29–41, 2002.

continued in next slide...

---



...from previous slide

---

- [13] A. M. Hershenson, S. Boyd, T. H. Lee, "CMOS operational amplifier design and optimization via geometric programming," in Proc. 1st Int. Workshop Design Mixed-Mode Integrated Circuits Application, Cancun, Mexico, pp. 15–18, 1997.
- [14] M. Hershenson, S. P. Boyd, T. H. Lee, "Optimal design of a CMOS opamp via geometric programming," IEEE Trans. Comp.-Aided Design of Intg. Circ. and Sys., vol. 20, no. 1, pp. 1–21, Jan. 2001.
- [15] C. C. Huang, S. H. Hung, J. F. Chung, "Front-end amplifier of low-noise and tunable B/W gain for portable biomedical signal acquisition", IEEE Circuits and Systems, pp. 2717–2720, 2008.
- [16] D. Yates, E. Lopez-Morillo, R. G. Carvajal, "A Low-Voltage LowPower Front-End for wearable EEG Systems", Conference of the IEEE EMBS, 2007.
- [17] L. Lentola, A. Mozzi, A. Neviani, A. Baschirotto, "A 1uA front-end for pacemaker atrial sensing channels", IEEE, 2009.
- [18] C. Bronskowski and D. Schroeder, "An ultra low–noise CMOS Operational Amplifier with programmable Noise Power Trade-off , " IEEE Solid-State Circ. Conference, pp. 368–371, 2006.
- [19] P. E. Allen and D. R. Holberg, "CMOS analog circuit design," Second Edition, Oxford University Press, 2002.
- [20] B. A. A. Antao, "Trends in CAD of analog ICs" IEEE Circ. Devices Mag. vol. 12, pp. 31–41, 1996.
- [21] L. R. Carley, R. A. Rutenbar, "How to automate analog IC designs," IEEE Spectr. 25, pp. 26–30, 1988.
- [22] S. Boyd, S. J. Kim, L. Vandenberghe, A. Hassibi, A tutorial on geometric programming. Technical Report, Stanford Univ. and Univ. of California (2005). <http://www.stanford.edu/~boyd/gptutorial.html>
- [23] P. Mandal, V. Visvanathan, "CMOS op-amp sizing using a geometric programming formulation," IEEE Trans. Comput. Aided Des. Integr. Circ. Sys. vol. 20, pp. 22–38, 2001.
- [24] S. Boyd, L. Vandenberghe, Introduction to Convex Optimization with Engineering Applications (Stanford University, Stanford, 1997. <http://www.stanford.edu/~boyd/cvxbook>
- [25] M. Hershenson, S. M. Sunderajan, Automated circuit design using active set solving process. US 8307309 B1, (2012), <http://www.google.co.uk/patents/US8307309>

continued in next slide...

---



...from previous slide

---

- [26] D. Binkley, M. Bucher, and D. Foty, "Design-oriented characterization of CMOS over continuum of inversion level and channel length," Proc. 7th IEEE Int. Conf. on Electronics, Circuits & Systems, Kaslik, Lebanon, pp. 161–164, 2000.
- [27] C. Enz, F. Krummenacher, E. Vittoz, "An analytical MOS transistor model valid in all regions of operation and dedicated to low-voltage and low-current applications," J. AICSP, 8, pp. 83–114, 1995.
- [28] F. Silveira, D. Flandre, P. G. A. Jespers, "A ( $gm/ID$ ) based methodology for the design of CMOS analog circuits and its application to the synthesis of a silicon-on-insulator micropower OTA," IEEE J. SolidState Circ., 31, pp. 1314–1319, 1996.
- [29] D. Foty, M. Bucher, D. Binkley, "Re-interpreting the MOS transistor via the inversion coefficient and the continuum of  $gms/ID$ ," Proc. Int. Conf. on Electronics Circ. & Sys., pp. 1179–1182, 2002.
- [30] A. Cunha, M. Schneider, C. G. Montoro, "An MOS transistor model for analog circuit design," IEEE J. Solid State Circ., vol. 33, pp. 1510–1519, 1998.
- [31] B. K. Ahuja, "An improved frequency compensation technique for CMOS operational amplifiers," IEEE J. Solid-State Circ., vol. 18, pp. 629–633, Dec. 1983.
- [32] M. Goswami, S. Kundu, "Constrained low-power CMOS analog circuit design via all-inversion region MOS model," Proc. 4th IEEE Int. Conf. on Consumer Electronics ICCE-Berlin, pp. 277–278, Berlin, Germany, Sept. 2014.
- [33] M. Goswami, S. Kundu, "Constrained optimization of CMOS analog circuits via all-inversion region MOS model," Proc. Int. Conf. on Computational Advancement in Communication Circ. and Sys. ICCACCS, Agarpara, India, Oct. 2014 and Journal Lecture Notes in Electrical Engineering LNEE, Springer [ISSN: 1876-1100].
- [34] M. Goswami, S. Kundu, "Design and analysis of semi-empirical model parameters for short-channel CMOS devices," International Journal of Soft Computing and Engineering IJSCE [ISSN: 2231-2307], vol. 4, issue 3, pp. 86–89, July 2014. Available: <http://www.ijsce.org/attachments/File/v4i3/C2317074314.pdf>



# DZIĘKUJĘ

---

---

## QUESTIONS / SUGGESTIONS

