PRINCIPLES and PRACTICE of RADIATION ONCOLOGY

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OUTLINE

- Physical basis
- Biological basis
- History of radiation therapy
- Treatment planning
- Technology of treatment delivery
- Future directions

Radiation

Ionizing Non-ionizing Indirectly **Directly** visible light IR, UV Charged x-rays, **Particles** gamma, neutrons

Ionizing Radiation: X-rays

Result from extranuclear processes

- characteristic radiation

- bremsstrahlung radiation

Ionizing Radiation: Gamma Rays

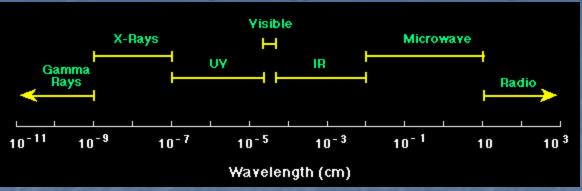
Intra nuclear process (RADIOISOTOPE)

- unstable (radioactive) nucleus decays towards ground state
- parameters characterizing decay:
 t_{1/2}, decay constant, specific activity

Common Radioisotopes

<u>Isotope</u>	<u>Half-Life</u>	<u>Energy</u>
Co-60	5.26 yr	1.25 MeV
Cs-137	30 yr	0.661 MeV
I-125	60 d	28 keV
Pd-103	17 d	21 keV

X Rays (photons)



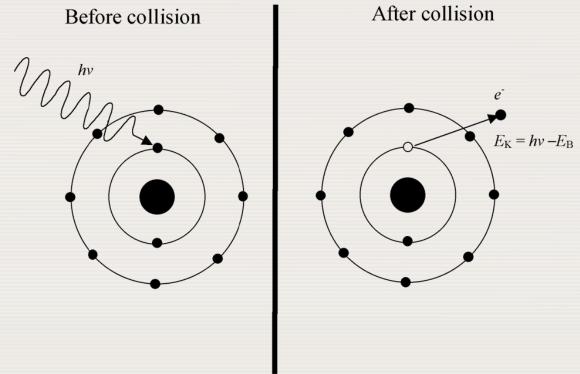
- Interact with matter in well characterized mechanisms:
 - photoelectric interaction
 - Compton interaction
 - pair production

Infinite range, probability-based interactions

1.4 PHOTON INTERACTIONS

1.4.4 Photoelectric effect

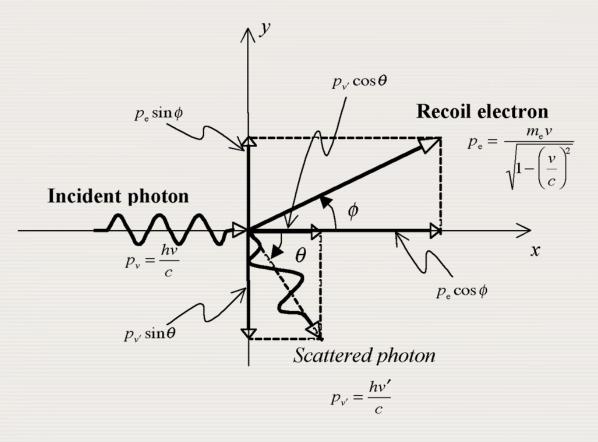
- Schematic diagram of the photoelectric effect
 - A photon with energy $h\nu$ interacts with a K-shell electron
 - The orbital electron is emitted from the atom as a photoelectron





1.4 PHOTON INTERACTIONS

1.4.6 Compton scattering



Conservation of energy

$$hv + m_{\rm e}c^2 = hv' + m_{\rm e}c^2 + E_{\rm K}$$

Conservation of momentum (x axis)

$$p_{v} = p_{v} \cos \theta + p_{e} \cos \phi$$

Conservation of momentum (y axis)

$$0 = -\boldsymbol{p}_{v'} \sin \theta + \boldsymbol{p}_{e} \sin \phi$$

Compton expression:

$$\Delta \lambda = \lambda_{\rm c} (1 - \cos \theta)$$

$$\lambda_{\rm c} = \frac{h}{m_{\rm e}c} = 0.24 \ \Box$$



1.4 PHOTON INTERACTIONS

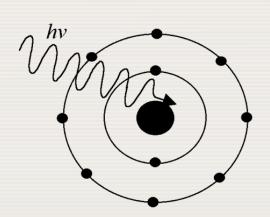
1.4.7 Pair production

- In pair production
 - The photon disappears.
 - An electron-positron pair with a combined kinetic energy equal to $hv-2m_ec^2$ is produced in the nuclear Coulomb field.
 - The threshold energy for pair production is:

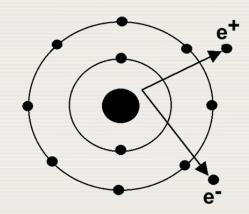
PAIR PRODUCTION

$hv_{\text{thr}} = 2m_{\text{e}}c^2 \left\{ 1 + \frac{m_{\text{e}}c^2}{M_{\text{A}}c^2} \right\} \approx 2m_{\text{e}}c^2$

Before collision



After collision



m electron mass

M_A mass of nucleus

 $m_{\rm o}c^2 = 0.511 \, {\rm MeV}$



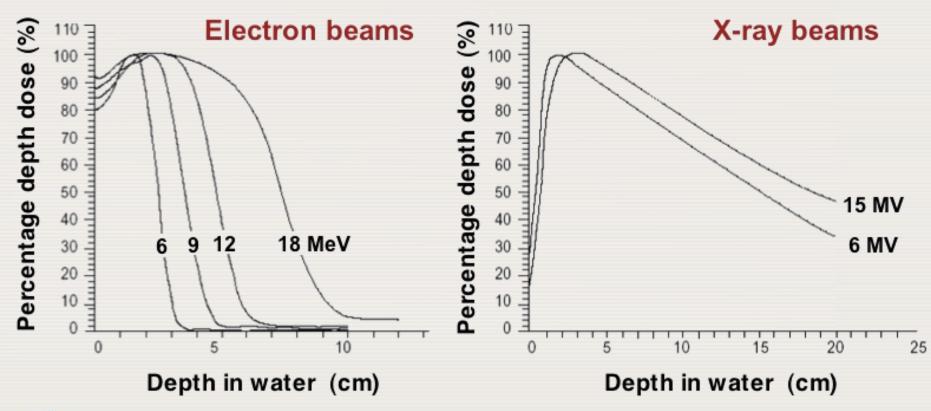
Charged Particles

Interact via collisional and radiative mechanisms

Predictable finite range

CENTRAL AXIS DEPTH DOSE DISTRIBUTIONS

The general shape of the central axis depth dose curve for electron beams differs from that of photon beams.





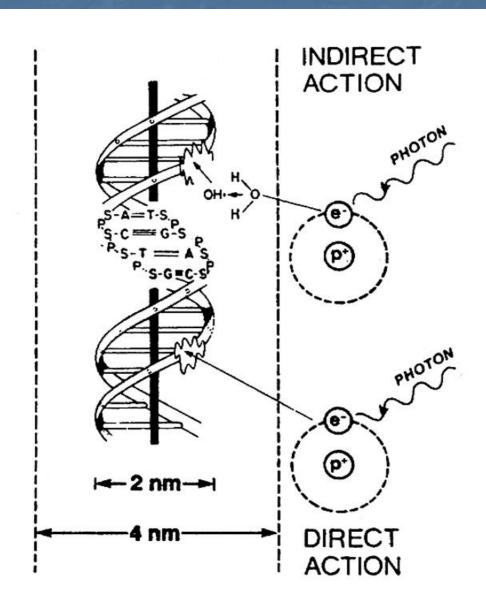
RadioBiology

- Physical deposition of energy leads to chain of reactions which ultimately lead to the observed clinical effect.
- Final energy transfer to material is via energetic electrons and positrons produced in a photon interaction.

Target Theory

- Cell killing is a multi-step process
- Absorption of energy in some critical volume is first step
- Deposition of energy as ionization or excitation in the critical volume leads to molecular damage
- Damage prevents normal DNA replication and cell division

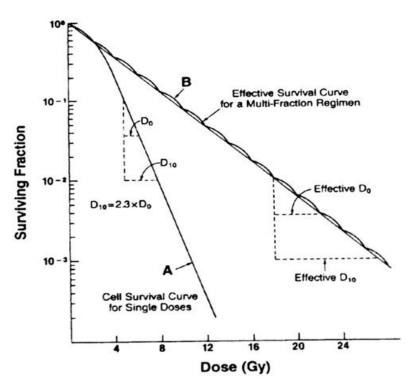
The two mechanisms of cell Kill



Cellular Response

- Loss of function
 - radiation mutagenesis and carcinogenesis
 - interphase cell death (apoptosis)
- Loss of reproductive ability

Cell Survival Curve



Curve A: Survival curve for mammalian cells. The dose required for to reduce survival by a factor of 10 (i.e. D_{10} is equal to 2.3 x D_0).

Curve B: Effective survival curve for cells exposed to a multifraction regimen, where doses are separated by a time interval sufficient for repair of sublethal damage. The effective survival curve is shallower than the single dose survival curve, i.e. D_0 effective is larger than D_0 . Again the D_{10} effective = 2.3xDo effective.

Cell Survival Curve (con't)

- Inherent radiosensitivity
- Oxygen concentration
- Repair processes
- Repair of potentially lethal damage (PLD)
- Cell cycle phase dependence
- Cell proliferation status

Parameters

- Linear Energy Transfer (LET)
 amount of energy deposited per unit path length
- Relative Biologic Effectiveness (RBE)
 measures efficiency of radiation in
 producing biological response relative
 to a standard radiation (250 kVp)

Parameters (con't)

- Oxygen Enhancement Ratio (OER)
 - oxygenated cells more sensitive to radiation damage
 - anoxic cells radioresistant
- Radioprotectors
- Radiosensitizers

Tumor Response

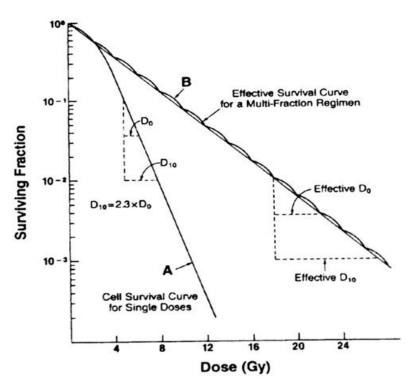
- Repair
- Repopulation
- Reoxygenation
- Reassortment

_ 4 R's of Radiobiology

Dose Fractionation

- Dividing a dose into a number of fractions
 - spares normal tissues
 - repair of sublethal damage
 - repopulation of normal cells
 - increases damage to tumor cells
 - reoxygenation can occur
 - reassortment into radiosensitive phases of cell cycle

Cell Survival Curve



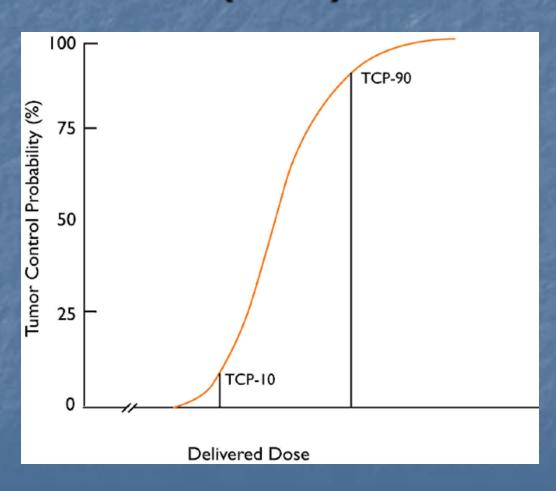
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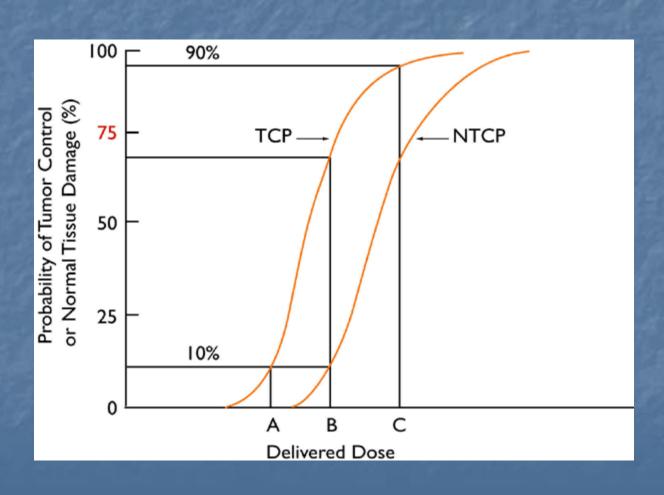
Tissue and Organ Response

- TCP Tumor Control Probability
 - likelihood of controlling tumor growth
- NTCP Normal Tissue Complication Probability
 - likelihood of normal tissue complications

Tumor Control Probability (TCP)



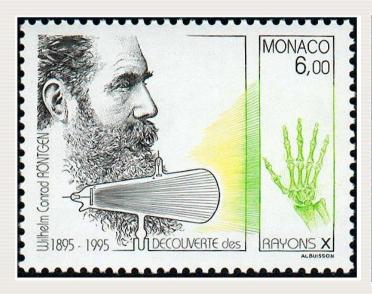
TCP vs. NTCP



Radiation Therapy History

- 1895 Roentgen discovers x-rays
- 1896 Becquerel discovers radioactivity (uranium)
- Biological effect of radiation evident almost immediately
- 1901 Pierre Curie self-induced radium burn on arm
- Early radiation therapy using radium (interstitial, intracavitary, surface applicators)

- The study and use of ionizing radiation in medicine started with three important discoveries:
 - X rays by Wilhelm Roentgen in 1895.
 - Natural radioactivity by Henri Becquerel in 1896.
 - Radium-226 by Pierre and Marie Curie in 1898.





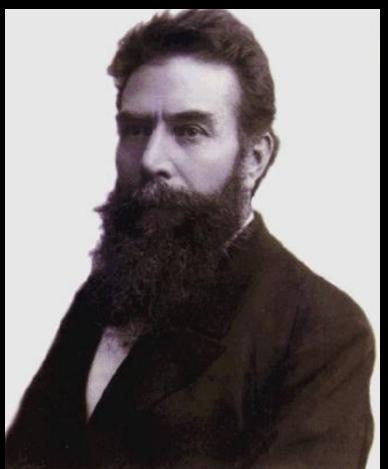




Discovery of X-rays

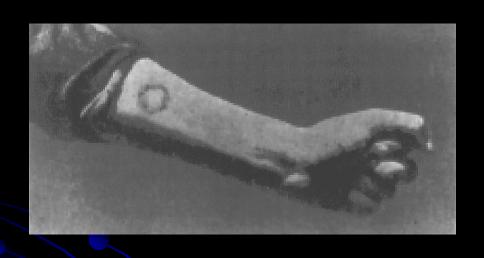
On 8 Nov 1895, Wilhelm Conrad Röntgen (accidentally) discovered an image cast from his cathode ray generator.







Guinea Pig Physicist!



- Self induced radiation burn on Pierre Curie's arm, 1901
- Experiment with biological application of radioactivity...first indication of biological effect?

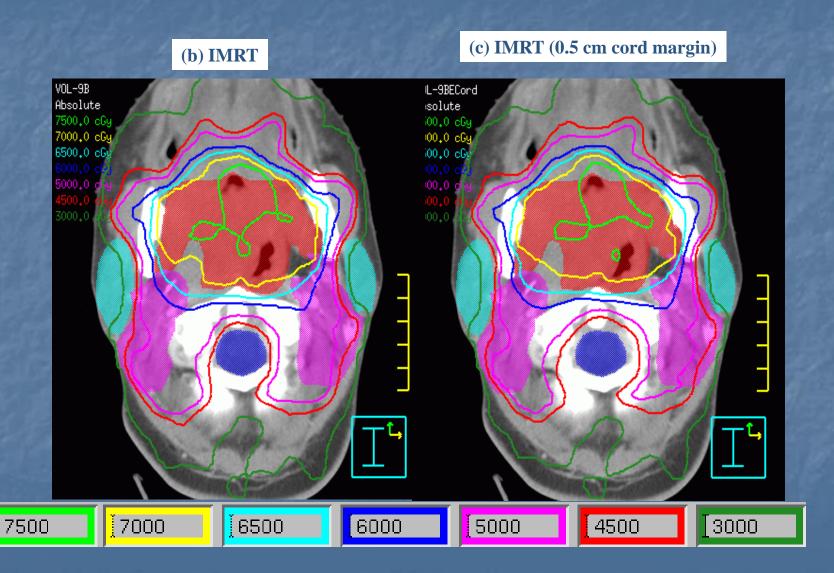


Early Radiation Therapy



- Early surface applicator,1922
- Lack of rigorous quantitative dosimetry
- Disregard for radiation safety procedures

IMRT plan: Head & Neck ca



Modern Radiation Therapy Team

- Radiation Oncologist / Resident
- Medical Physicist / Resident
- Dosimetrist
- Radiation Therapist
- Nurse
- Social Worker
- Administrator

Goal of radiation therapy

"concentrate dose to target tissues and minimize dose to healthy tissues"

Radiation Therapy

- Brachytherapy therapy at a short distance
 - sources placed directly into tumor volume
- Teletherapy therapy at a large distance
 - source outside body

Review of Brachytherapy Principles

- •Highly localized dose to target with sharp fall-off in surrounding tissues
- •The ultimate conformal therapy?
- Inherent inhomogeneity and hot spots



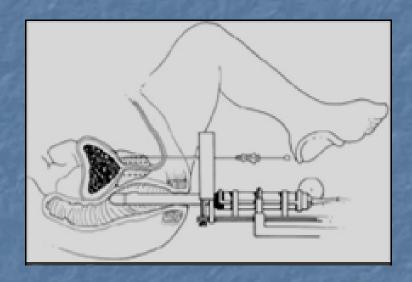
Brachytherapy Clinical Applications

- Historically, brachytherapy has been applied clinically to many anatomical sites
- e.g., eye, head and neck, brain, skin, bronchus/lung, esophagus, breast, prostate, female pelvis (gyn), soft tissue (sarcoma), and others...

Prostate Brachytherapy



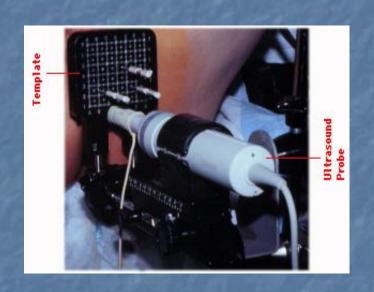
1970's MSKCC

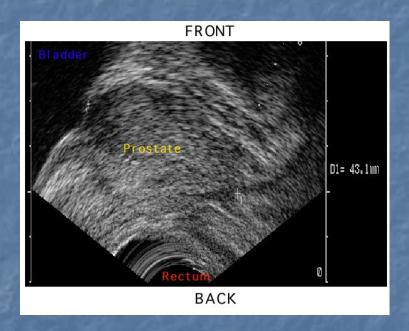


TRUS-guidance (early '90's)

Prostate Brachytherapy

TRUS Imaging and implant needle placement





Post-Implant Dosimetry

Post-implant imaging for verification and dosimetry



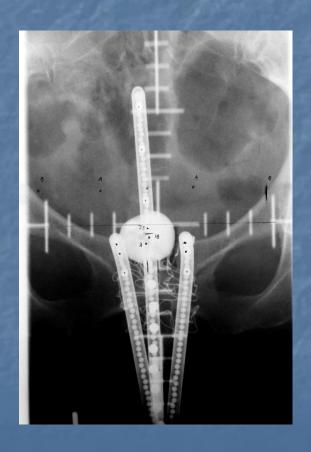


Plane Film (2D)

CT (3D)

GYN Brachytherapy

LDR Remote Afterloader procedure





Other Brachytherapy

HDR esophagus

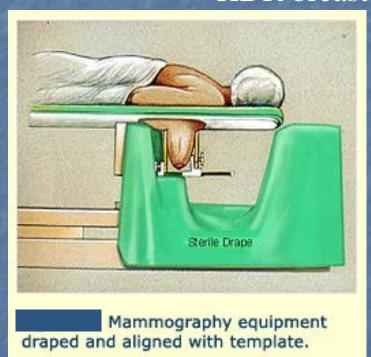


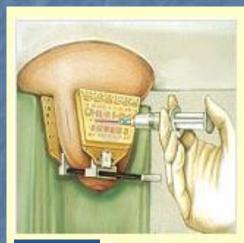


Typically 5 Gy/fx in 3-7 minutes

Other Brachytherapy

HDR breast





The breast under each hole is completely anesthetized prior to catheter insertion.

Teletherapy Energy Categories

- Superficial (10 80 kVp)
- Orthovoltage (100 500 kVp)
- Megavoltage (Co-60 35 MV)

Equipment for dose delivery

■ 1895 X-ray machine: Crookes type.

1913 X-ray machine: Coolidge type.

1940s Van de Graaff generator and betatron.

1950s Cobalt-60 teletherapy

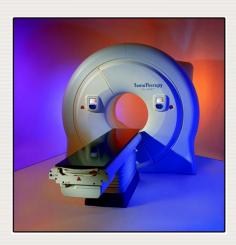
1960s Linear accelerator (linac) and Gamma Knife.

2000s Tomotherapy machine and Cyberknife.









Superficial / Orthovoltage (x-ray tube)



MEDICAL LINEAR ACCELERATOR



Patient flow in radiation therapy

- Consultation / Informed consent
- Conventional / Virtual simulation
- Treatment planning
- Simulation check / port film
- in vivo dosimetry

Imaging for target localization

1970s CT scanner

Allan Cormack

Godfrey Hounsfield

Nobel Prize 1979

1973 PET scanner

Edward J. Hoffman Michael E. Phelps

1980s MR scanner

Paul C. Lauterbur

Peter Mansfield

Nobel Prize 2003













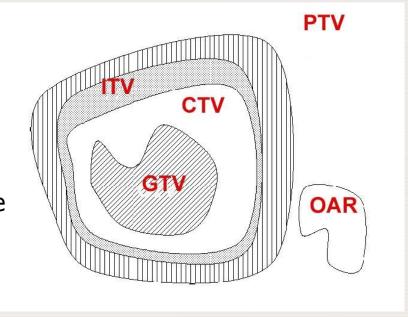
TREATMENT VOLUME DEFINITION

GTV – gross tumor volume palpable or visible extent of disease

CTV - clinical target volume GTV + subclinical microscopic disease

ITV - internal target volume CTV + margin for organ motion e.g., breathing

PTV - planning target volume
ITV + margin for setup errors and
treatment machine tolerances

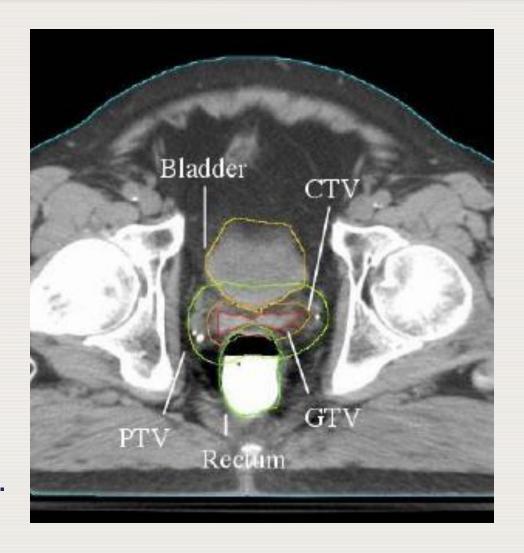




MALE PELVIC CONTOURING

Contours for different volumes have been drawn on this CT slice for a prostate treatment plan:

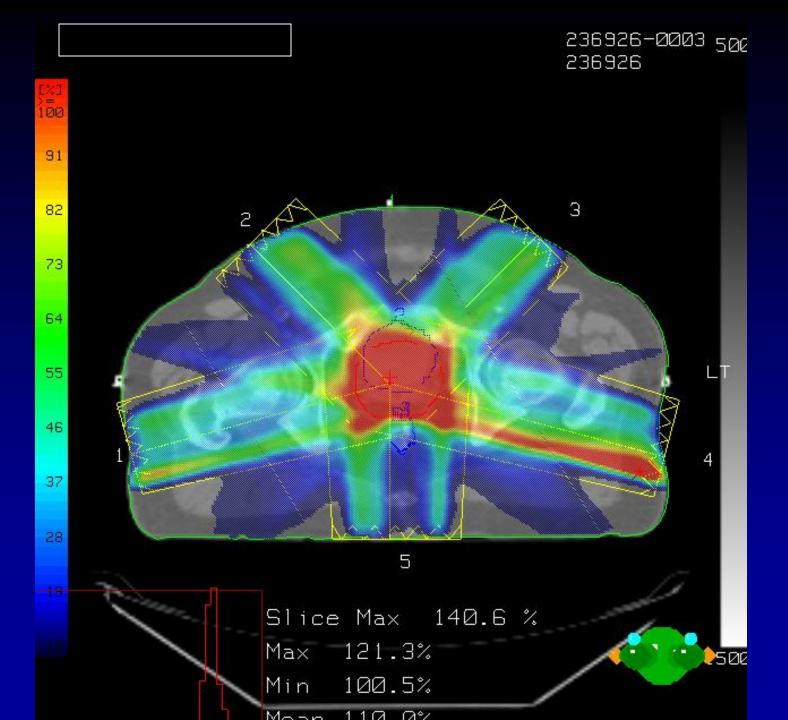
- GTV
- CTV
- PTV
- organs at risk (bladder and rectum).





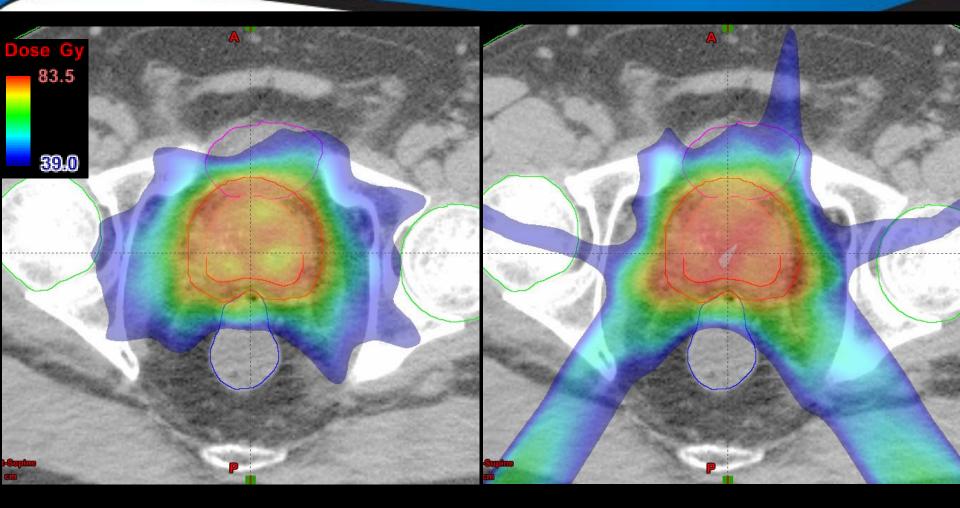
Treatment Planning







IMRT Quality



RapidArc Single arc IMRT

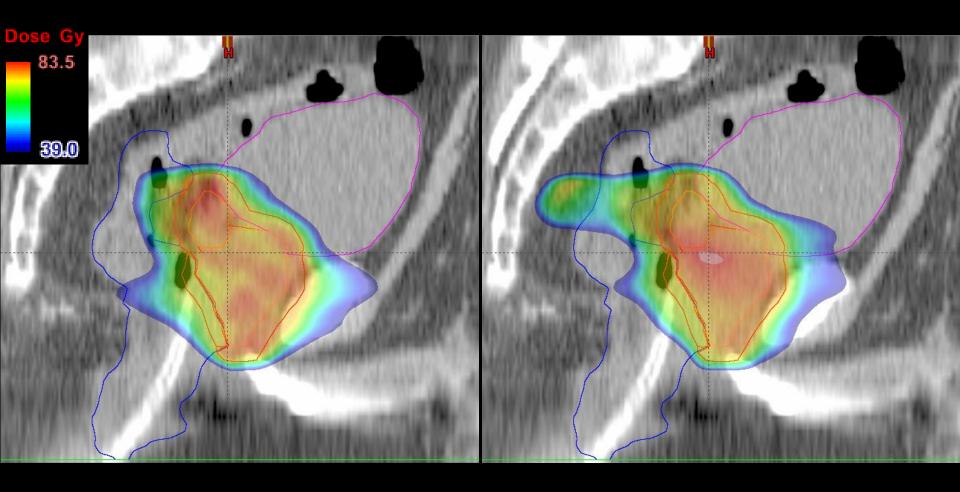
603 MU

Conventional 5-field IMRT

915 MU



IMRT Quality



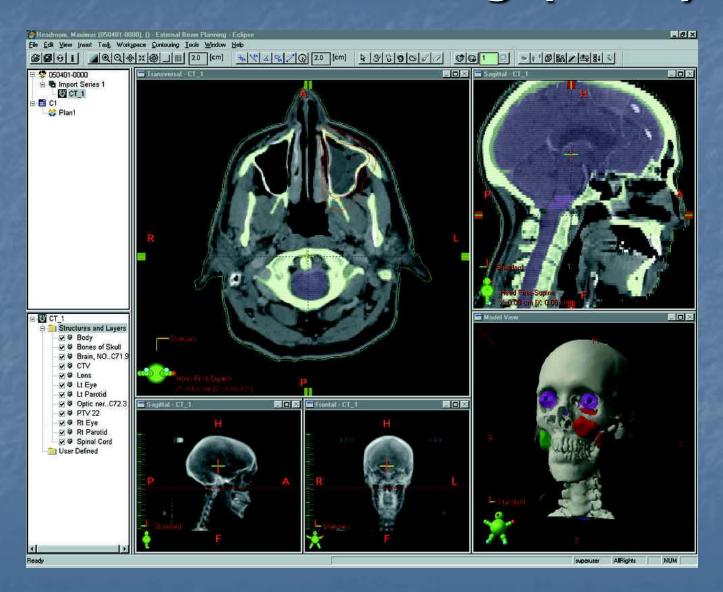
RapidArc Single arc IMRT

603 MU

Conventional 5-field IMRT

915 MU

Treatment Planning (con't)

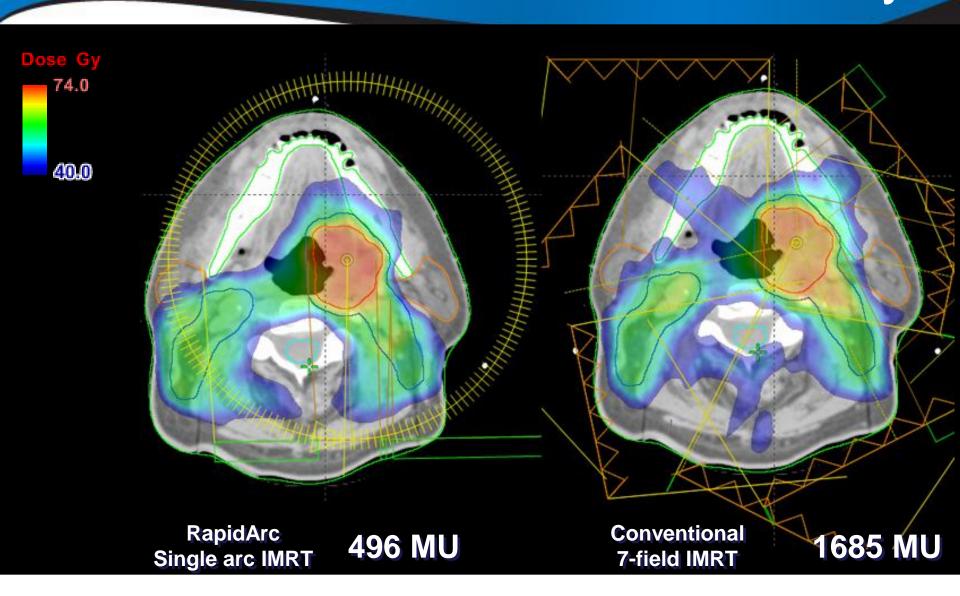


Radiation Therapy: State-of-the-art and future directions

- IMRT Intensity Modulated Radiation Therapy
- VMAT Volumetric Modulated Arc Therapy
- Tomotherapy Image at time of therapy

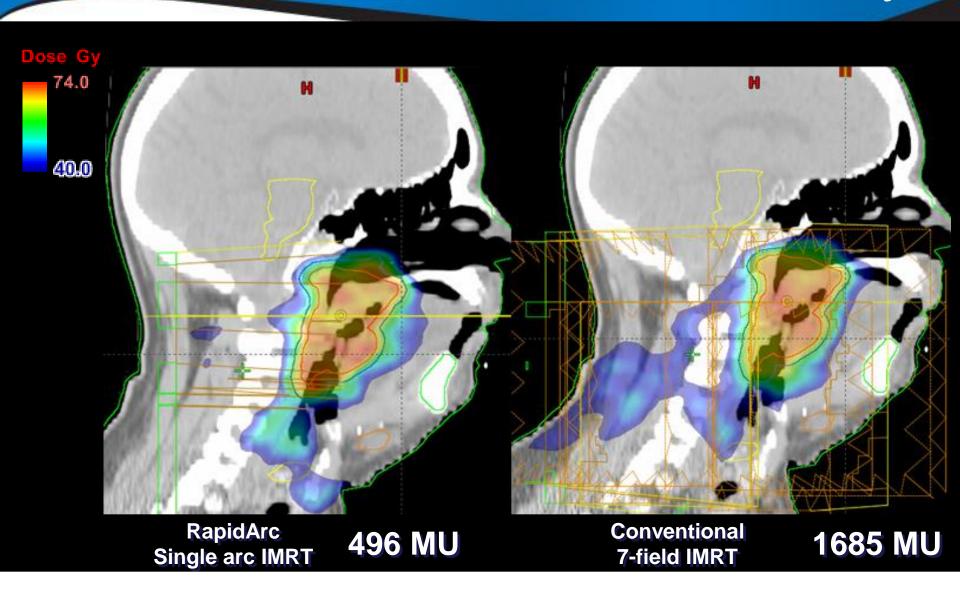


IMRT Quality





IMRT Quality



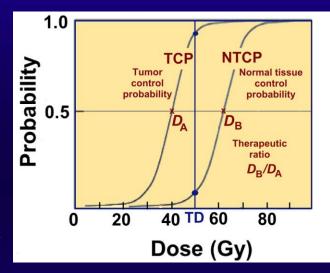
GOALS of MODERN RADIOTHERAPY

To improve tumor control

through an increase in tumor dose, i.e., through an increase in TCP

To reduce morbidity

through decreased dose to normal tissue, i.e., through a decrease in NTCP



Using

(1) More complex treatment techniques and

(2) New technology