

# A Carbon Nanotube Implementation of Temporal and Spatial Dendritic Computations

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**Abstract**—A neural dendritic computational circuit design is presented here. The circuit models the result of action potentials applied to biological synapses on a portion of a dendritic tree. The resultant excitatory post synaptic potentials (EPSPs) are combined in a dendritic tree that demonstrates linear, superlinear and sublinear summation of both spatially and temporally separated EPSPs. The synapse circuit models include neurotransmitter action, reuptake and membrane potentials. The output of the circuit is a combined Excitatory Post Synaptic Potential (EPSP). The circuit is simulated using carbon nanotube SPICE models. Variations of this design can be implemented to create a variety of dendritic computational subunits.

## I. INTRODUCTION

Within the neurons in the cortex, significant dendritic computations occur that affect the probability and frequency of neural firing. Action potentials arriving at the synapses create post-synaptic potentials on the dendritic arbor that combine in complex ways (e.g. [1], [2], [3]). There is growing consensus among neuroscientists that aspects of dendritic behavior contribute significantly to cortical functioning.

The biological synapse is complex, with controllable transmitters that can decrease or increase the excitability of the postsynaptic receptors. The activation probability of a given synaptic junction is regulated by the amount and timing of presynaptic and postsynaptic activity. Neurotransmitters must be present in sufficient amounts to develop post-synaptic potentials (PSPs), and the concentration of transmitters released can affect the height and duration of the PSP [4].

A second area of complexity is the ion channel, modeled biomimetically, e.g. by Hasler [5]. Ion channel conductance in turn affects membrane potential. Action potentials impinging on the synaptic cleft could result in temporal summation of the resulting PSPs, increasing the likelihood of the post-synaptic neuron eventually firing.

A third area of complexity involves the dendritic computations that occur on the EPSPs [6] [2]. These computations include linear, sublinear and superlinear additions whereas modeling inhibitory inputs is the subject of a future paper.

Carbon nanotubes may support the scale and interconnection density of a synthetic cortex. They are extremely small (a few nm. in diameter), current flow is largely ballistic (like the flow of electrons in free space), capacitances are in attofarads,

and rise and fall times in picoseconds. Appropriate interfaces can convert to biological signal levels and delays. Channel resistance is primarily due to the quantum resistance at the junction between the nanotubes and metallic connections, creating a challenge for analog circuit design. Carbon nanotubes have been shown to form dendritic structures, which may facilitate their use in synthetic neurons [7]. Finally, nanotubes have been shown to induce minimum immune system reactions in living tissue, making prosthetic devices with carbon nanotubes desirable [8].

We designed and simulated a carbon nanotube transistor circuit model of a neural synapse that captures, in a coarse manner, the actions of neurotransmitters, ion channel mechanisms, and temporal summation of PSPs. We have focused on excitatory PSPs (EPSPs) first, and have chosen economy of size over exact replication of waveforms, to facilitate scaling to cortical-sized biomimetic structures.

We have constructed a voltage adder [9] to implement some dendritic computations, and have simulated this circuit using carbon nanotube SPICE models. This adder is tunable to support sublinear to superlinear summations of PSPs. We have constructed a small portion of a dendritic arbor, and shown how action potentials impinging on the presynaptic terminals of the arbor produce output PSPs that are a function of the EPSPs invoked at each synapse of the arbor.

## II. BACKGROUND

Many electronic neurons have biomimetic features (e.g. [10]). The most notable research includes Mead's artificial retina [11]. This significant work originated with Mahowald and Mead [12], followed by Boahen [13] [14] and more recently Hasler [5]. Hynna and Boahen report on a circuit that generates a calcium spike with attention paid to exact replication of waveforms, and describe incorporation of the calcium spike circuit in an entire neuron circuit [15]. Some mixed-signal electronic models close to biological neurons include Liu and Frenzel's spike train neuron, with a 10-transistor mixed-signal synapse [16], and Pan's bipolar neuron [17]. An 8-transistor CMOS synapse [18] is close in scale and nature to our synapse, although they plan to use the synapse for summation of inputs from many pre-synaptic sites. Analog synapses have been reported by Pinto et al. [19] and Lee et al. [20] and a phase-lock loop synapse has been reported by Volkovskii [21]. The strength of our model and similar models is the correspondence between individual circuit elements and

specific physiological mechanisms in the biological neuron that allows us to vary synapse behavior easily with control inputs. This, and our choice of carbon nanotube technology, differentiates this work.

Elias modeled dendritic computations as early as 1992 [22]. Hasler and Farquhar also model dendritic transmission [5], [10], as do others (e.g. Arthur [23] and Rasche [24]). Existing cable models could be integrated with our computations for a complete dendritic model.

Single-walled carbon nanotubes avoid most of the fundamental scaling limitations of silicon, making them suitable for a synthetic cortex [25]. Liu, Han and Zhou have demonstrated directional growth of high-density single-walled carbon nanotubes on a- and r-plane sapphire substrates over large areas [26]. This technique may enable registration-free fabrication of nanotube devices and lead to integrable and scalable nanotube systems, including synthetic cortex circuits. They have developed a novel nanotube-on-insulator (NOI) approach, and a way to transfer these nanotube arrays to flexible substrates.

Efforts have been made in recent years on modeling CNFETs [27] [28] and CNT interconnects [29] [30], to evaluate the potential performance at the device level. Most of the reported models to date used a single lumped gate capacitance and ideal ballistic model to evaluate the dynamic performance [31] [32]. To evaluate CNFET circuit performance with improved accuracy, a CNFET device model with a more complete circuit-compatible structure and including the typical device non-idealities was constructed [33]. This recent publication presents a novel circuit-compatible compact SPICE model for short channel length (5nm 100nm), quasi-ballistic single wall carbon nanotube field-effect transistors (CNFETs).

### III. THE CARBON NANOTUBE SYNAPTIC CIRCUIT

The carbon nanotube synaptic circuit [34] [35] is shown in Figure 1. Action potentials (see Figure 2) arrive from the presynaptic neuron and terminate in our synaptic circuit. The simple action potential used here is an approximation of a typical biological action potential [36]. An incoming action potential will cause the potential in the synaptic cleft to rise. The PFET limits the peak amplitude of the synaptic cleft potential by turning off before the synaptic cleft potential rises to Vdd. The synaptic cleft potential in the electronic neuron (Figure 1) models the biological release of neurotransmitters stored in the presynaptic neuron into the cleft, where they bind to receptor proteins on the recipient (postsynaptic) neuron, causing the potential across the postsynaptic neural membrane to change. Once the neurotransmitters are released from the presynaptic terminal and bound in the postsynaptic terminal, they will be cleared from the synaptic cleft for reuse by reuptake mechanisms modeled via the pull-down network attached to the synaptic cleft [4].<sup>1</sup> The re-uptake control

<sup>1</sup>Since the SPICE model used in this study is geared toward short gate length transistors with near-ballistic transport, we use three transistors in series to model the resistance that represents the reuptake delay. The quantum contact resistances of the three transistors are added in series.

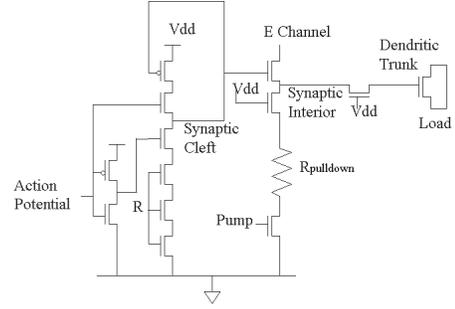


Fig. 1. The Carbon Nanotube Synaptic Circuit

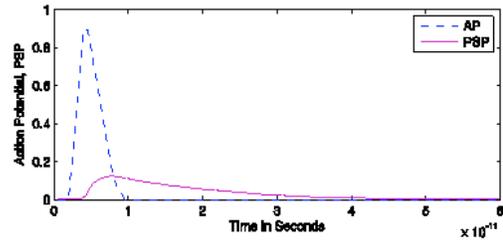


Fig. 2. The Action Potential and PSP at the Dendritic Trunk under Normal Operation

voltage,  $R$  allows the efficiency of the reuptake mechanism to be tuned. The action potential is inverted and used to block pull down of the synaptic cleft potential to delay reuptake of the neurotransmitter at the presynaptic neuron while there is a positive action potential. Reuptake can be inhibited or slowed by lowering the reuptake control voltage  $R$ .

The increase in potential in the synaptic cleft will temporarily turn on the transistor connected to the ion electromotive force control,  $E$  Channel, causing the potential at Synaptic Interior to rise. This models the change in biological membrane potential due to the increased conductance of neurotransmitter gated ion channels and the subsequent influx of charge carrying ions (e.g. sodium). A tunable pull-down network<sup>2</sup> controls the cell interior's return to resting potential (steady state).

The synaptic interior potential is transferred through a resistive connection to the dendritic trunk, which carries the postsynaptic potential (PSP) to the neuron cell body. The weight control allows the importance of this synapse to be tuned with learning. The dendrite trunk terminates on the gate of a single test load NFET that is removed when the synapse is connected to other neural components.

In the archetypical biological neuron we are modeling, potentials range from around  $-75\text{mV}$  to  $+40\text{mV}$  with action potentials peaking around  $+40\text{mV}$ . Since the carbon nanotube synapse is designed to operate with  $V_{\text{dd}}$  around  $0.9\text{V}$  and with  $0.0\text{V}$  (Ground) as the resting potential, the potentials were scaled accordingly, with  $0\text{V}$  circuit potential corresponding to  $-75\text{mV}$  biological potential and  $0.9\text{V}$  circuit potential corre-

<sup>2</sup>Three transistors in series provides the  $R_{\text{pulldown}}$  resistance.

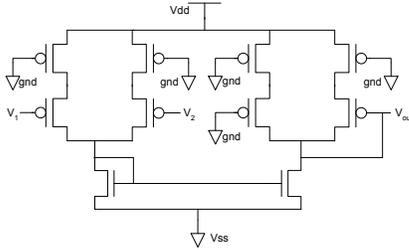


Fig. 3. The Voltage Adder

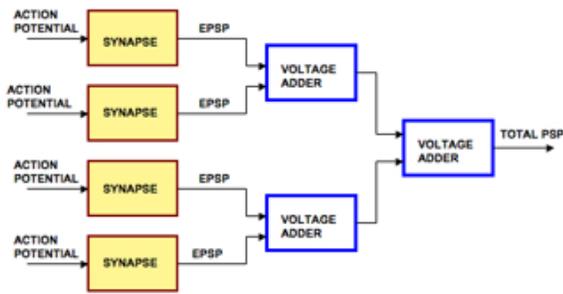


Fig. 4. The Dendritic Arbor Portion

sponding to 40mV biological potential. Likewise, the speed of the carbon nanotubes allowed us to scale the delays with about 1 ms in the biological neuron scaling to about 2 ps in the nanotube neuron [36].

#### IV. THE VOLTAGE ADDER AND DENDRITIC ARBOR

The adder circuit [9] is shown in Figure 3. A block diagram of the dendritic arbor portion is shown in Figure 4. There are four synapses in the arbor, each on a separate dendritic branch.

#### V. EXPERIMENTS WITH THE DENDRITIC ARBOR CIRCUIT

We performed several experiments with the dendritic arbor circuit. First, we simulated four synapses in the dendritic arbor excited with action potentials arriving at the same time, with linear addition. Then we simulated the addition of two synapses with action potentials arriving at varying times. For the third phase of the simulations, we varied the additions to be sublinear and superlinear. Finally we simulated the dendritic arbor with some PSPs weakened as a result of reduced neurotransmitter concentration (modeled by decreasing the source voltage on the PMOS pull up transistor in the synapse).

The postsynaptic potential appearing at the dendritic trunk is shown in Figure 2. This potential is approximately 14% of the action potential and the duration is about 6 times as long as the action potential, similar to EPSPs described in the literature.

In the first experiment, we tuned the dendritic PSP adders by adjusting transistor sizes to be linear, and all four synapses

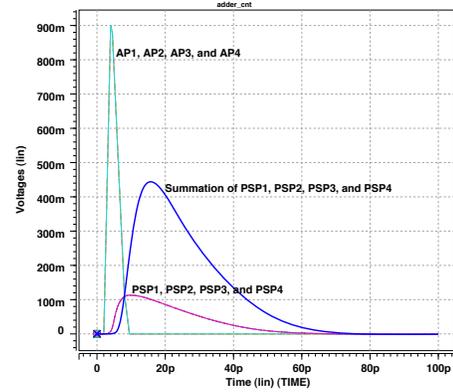


Fig. 5. The Summation of Four EPSPs in the Dendritic Arbor: AP indicates Action Potential

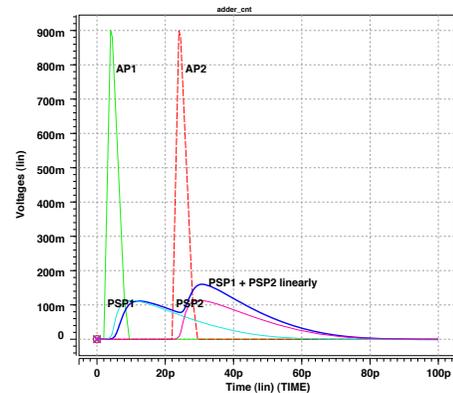


Fig. 6. The Temporal and Spatial Summation of Two EPSPs Excited by Action Potentials Arriving at Different Times

were excited simultaneously, as shown in Figure 5. In the second experiment, we simulated two action potentials (APs) arriving at staggered times so that the two EPSPs peaked at different times, demonstrating temporal and spatial summation. The resultant total EPSP is shown in Figure 6. A third experiment shows the types of PSP computation possible using our circuitry: superlinear, sublinear and linear, shown in Figure 7. The final experiment (Figure 8) illustrates the summation of weak and strong EPSPs.

#### VI. CONCLUSIONS

A typical carbon nanotube synapse has been designed and simulated using SPICE. This synapse has been replicated and used in a portion of a dendritic arbor to illustrate some varieties of dendritic computations that occur. The dendritic computation shown is one of several types of computations that occur.

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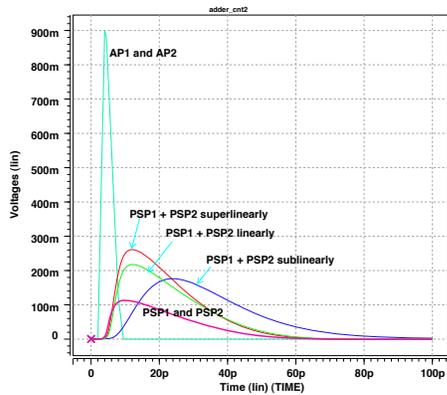


Fig. 7. EPSPs Summed Linearly, Sublinearly, and Superlinearly

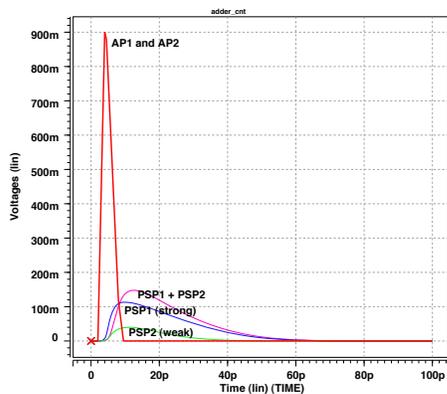


Fig. 8. Summation of Weak and Strong EPSPs

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